THE WAKE DYNAMICS AND FLIGHT FORCES OF THE FRUIT FLY
DROSOPHILA MELANOGASTER

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Accepted 20 May 1996

Summary

We have used flow visualizations and instantaneous force measurements of tethered fruit flies (Drosophila melanogaster) to study the dynamics of force generation during flight. During each complete stroke cycle, the flies generate one single vortex loop consisting of vorticity shed during the downstroke and ventral flip. This gross pattern of wake structure in Drosophila is similar to those described for hovering birds and some other insects. The wake structure differed from those previously described, however, in that the vortex filaments shed during ventral stroke reversal did not fuse to complete a circular ring, but rather attached temporarily to the body to complete an inverted heart-shaped vortex loop. The attached ventral filaments of the loop subsequently slide along the length of the body and eventually fuse at the tip of the abdomen. We found no evidence for the shedding of wing-tip vorticity during the upstroke, and argue that this is due to an extreme form of the Wagner effect acting at that time.

The flow visualizations predicted that maximum flight forces would be generated during the downstroke and ventral reversal, with little or no force generated during the upstroke. The instantaneous force measurements using laser-interferometry verified the periodic nature of force generation. Within each stroke cycle, there was one plateau of high force generation followed by a period of low force, which roughly correlated with the upstroke and downstroke periods. However, the fluctuations in force lagged behind their expected occurrence within the wing-stroke cycle by approximately 1 ms or one-fifth of the complete stroke cycle. This temporal discrepancy exceeds the range of expected inaccuracies and artifacts in the measurements, and we tentatively discuss the potential retarding effects within the underlying fluid mechanics.

Key words: vortex wake, insect flight, aerodynamics, Drosophila melanogaster.

Introduction

As a flying animal moves through the air, it generates aerodynamic forces with its wings and leaves behind a distinct wake. These two processes are inextricably linked, since any aerodynamic force produced by an animal requires an equal and opposite change in fluid momentum. Consequently, the goal of understanding the production of aerodynamic forces may be approached from either of two directions: by studying the time course of force generation by the flapping wings or by characterizing the structure of the resultant wake. These methods are not mutually exclusive, but are instead different approaches to the same problem.

The derivation of mean flight forces from the wake is the underlying basis for the vortex theories of Ellington (1984c) and Rayner (1979a,b), which both use elaborations of the Rankine–Froude theory of propellers to calculate the steady rate of change of fluid momentum. These theories are simple and robust since they do not require any precise knowledge of the kinematics. By the same token, however, they cannot be used to predict the time history of force generation and offer no direct insight into the underlying aerodynamic mechanisms.

Traditional approaches to the study of aerodynamics focus not on fluid momentum per se, but rather on the means by which the wings generate forces. The basis of the Kutta–Joukowski theory is a direct proportionality between lift and the bound circulation generated by the motion of a wing. It has the crucial disadvantage of being based almost exclusively on steady-state assumptions, which give it limited utility in studies of animal flight. There are, however, an increasing number of theories that consider unsteady mechanisms by which wings generate forces in ways that do not require bound circulation (Maxworthy, 1981; Wu et al. 1991; Spedding, 1992; Dickinson and Götz, 1993; Dickinson, 1994; Ellington, 1995). Together, these theories of airfoil function may eventually offer a framework for assessing the consequences of differences in wing morphology and kinematics – a feature that is missing from approaches that emphasize wake momentum alone.

In spite of the experimental difficulties inherent in visualizing wake structure and making direct measurements of instantaneous flight forces, a cohesive image of force
generation and wake structure in birds, bats and insects has begun to emerge. Early flow visualizations confirmed that hovering and slow-flying birds generate a single vortex ring during each wing stroke (Kokhshaysky, 1979; Spedding et al. 1984). However, careful quantification of the vortex ring momentum generated by flying birds failed to account for all the forces necessary to sustain flight (Spedding, 1986). This discrepancy may be due to changes in the momentum of the wake that are difficult to visualize. In contrast to the discrete vortex rings produced in hovering flight, the vortex filaments shed from the two wing tips during fast forward flight do not join at the end of the downstroke, but rather give rise to two continuous vortex tubes trailing behind the animal (Rayner et al. 1986; Spedding, 1987). Although many of the earlier wake reconstructions were carried out on birds and bats, a number of exquisite flow visualizations have recently been performed on insects (Brodsky, 1991, 1994; Grodnitsky and Morozov, 1992, 1993). These wake patterns are similar to those of hovering birds, although in some examples the vortex rings of the downstrokes are linked with one another via the tip vortices of a force-generating upstroke, producing a linked vortex chain (Brodsky, 1994). Insects, such as the crane fly Tipula paludosa, with sufficient wing separation during both dorsal and ventral stroke reversal appear to make a separate vortex chain behind each wing (Brodsky, 1991). Owing to limitations in temporal resolution, flow visualization studies have emphasized insects that operate at relatively low wingbeat frequencies. Much less is known of the wake structure in such accomplished fliers as bees, wasps and flies, which employ high wingbeat frequencies. In addition, all the species examined so far fly at relatively high Reynolds numbers. In this paper, we present a wake reconstruction for the fruit fly, Drosophila melanogaster, with a wingbeat frequency of approximately 200 Hz operating at an intermediate Reynolds number of approximately 100.

Compared with a relatively rich collection of flow visualization studies, calibrated measurements of instantaneous flight forces for flying animals are quite scarce. Cloupeau et al. (1979) compared instantaneous lift measurements in locusts with Jensen’s (1956) measurements of lift coefficients on isolated wings and concluded that unsteady mechanisms must augment force production. More recently, Wilkin and colleagues have reached similar conclusions in measurements of instantaneous flight forces of both locusts and moths (Wilkin, 1990, 1991; Wilkin and Williams, 1993). Wolf (1993), although unable to account for inertial forces, has correlated changes in the dynamics of lift within each wing stroke of a locust to changes in the activity of specific flight muscles. Three force recordings have been made using flies (Buckholz, 1981; Zanker and Götz, 1990; G. Nalbach, unpublished results), but these recordings were either uncalibrated or did not account for inertial forces. Although few in number, these experiments provide essential data for testing models of force generation in insect flight.

At some level, the two methods of inquiry, flow visualization and force measurement, must meet to form a cohesive picture. The pressure differential that generates lift according to the Kutta–Joukowski theory is simply another manifestation of the momentum impulse of a growing vortex ring (Milne-Thomson, 1966). The main purpose of this study is to integrate both analyses on the same animal in the hope of constructing a more synthetic view of force generation in flight.

Materials and methods
Flow visualization
The arrangement for visualizing the wake of a tethered fruit fly is indicated in Fig. 1A. Animals were mounted onto a tungsten rod using light-activated cement (GlasKleber, Loctite) and placed within the open working section of a 17 mm diameter wind-tunnel that produced a laminar flow of 20 cm s$^{-1}$. We aligned the fly within an optical wingbeat analyzer which produced a TTL pulse each stroke during the ventral flip rotation (Götz, 1987; Dickinson et al. 1993). Lycopodium spores, hollow spheres of approximately 30 μm diameter, were introduced upstream of the fly within the wind-tunnel and illuminated with a 0.6 mm thick sheet of light from a line-generating diode laser (670 nm, 4 mW). The exposure time was controlled by providing current to the laser diode for a specified amount of time. The laser source and line-generating optics were mounted on a micromanipulator so that the light slice could be moved to illuminate different portions of the wake (Fig. 1B,C). Images of particle trajectories were captured using a Peltier-cooled CCD camera (Photometrics) and stored on a Macintosh Quadra 800 computer for analysis. The Reynolds number for a slowly flying Drosophila is approximately 100, which is several orders of magnitude below the turbulent transition for a flat plate. For this reason, we expected that all the flows produced by the wings would be laminar.

The animals were tethered in the air flow at a body angle of approximately 20° with respect to the oncoming flow. The angle of the longitudinal body axis during free flight at an airspeed of 20 cm s$^{-1}$ is expected to be approximately 50° (see section on force measurements). Therefore, the orientation of the flies in our experiments was not exactly equivalent to free-
flight conditions. The low body angles at which we tethered the animals in both the flow visualization and interferometry experiments were required in order to maintain the wing stroke plane at an inclination that would produce accurate triggering of the wingbeat analyzer. However, we do not think that this discrepancy is likely to have significant effects on the flow pattern for several reasons. The advance ratio for our tethered flies (calculated according to Ellington, 1984a) was 0.04.
approximately 0.085, which indicates that the flows are dominated by the beating of the wings and not by the background air velocity of the wind-tunnel. The average sectional wing velocity in Drosophila is 125 cm s⁻¹, in a stroke plane that is inclined at approximately 70° with respect to the body axis. From these values, it is possible to estimate that at a tunnel velocity of 20 cm s⁻¹, the 30° error in the placement of the body angle would cause only a 4% decrease in the downstroke velocity of the wing and a comparable increase in the upstroke velocity. Further, as described in the Results section, the mean flight forces measured in still and moving air were not statistically different from one another. Thus, despite a body angle that is lower than normal, we believe that our tethered configuration approximates near-hovering conditions.

We collected data only from individuals that produced stable flight sequences and displayed the leg posture typical of free flight. Flies that exhibited short flight bouts and frequent landing responses after tethering were discarded. We generated both long- and short-exposure images of the particle flow in the fly’s wake. Long exposures (30 ms) were used to visualize the gross structure of the wake over several wingbeat cycles. Shorter exposures (0.5–1 ms) were used to visualize flow dynamics within a single stroke cycle. The wingbeat analyzer generated a TTL pulse during the ventral flip of each wing stroke, which we used to trigger the CCD exposure. By varying the delay between the ventral flip pulse and the camera exposure, we could acquire images of the flow at different phases of the wingbeat cycle. Typically, four separate phase-locked images were superimposed on a single frame. This allowed us to examine a reasonable number of particle streaks without the necessity of bombarding the fly with an excessive density of Lycopodium spores for each exposure. These composite images, which were acquired over many different stroke cycles, could then be used to generate a phase-reconstructed film of the wake dynamics within a single wingbeat. Quantitative analysis of the flow images was accomplished by measuring the length and direction of individual particle streaks and analyzing the resultant vector fields using the software program Transform (Spyglass).

**Force measurements**

The apparatus for measuring instantaneous forces is illustrated in Fig. 1D. The fly was tethered at the anterior notum to a 60 mm long, 0.1 mm diameter steel wire which was tuned to a frequency of 4.0 kHz (with the attached fly). To measure the displacement of the wire along one of the main axes, a stationary shim was adjusted so as to leave a gap of 0.11 mm between its edge and the adjacent boundary of the wire. The wire’s opposite boundary was concealed behind the edge of another shim (not shown in Fig. 1). A frequency-modulated beam from a diode laser (670 nm, 2.5 mW) was aimed through the gap to generate an interference pattern. The displacements of the wire relative to the fixed shim were transduced by a pair of photodiodes positioned 1.1 m away. We centered the two diodes on the intensity inflection points of the third minimum of the interference pattern, which was located approximately 20 mm from the central beam. The motion of the interference minimum enlarged the displacement of the wire by a factor of 180 and was transduced by the demodulated differential signal of the photodiodes. This differential signal could be calibrated as deflection force. Two sets of interferometry components (shims, laser, detector) were used in order to detect two orthogonal forces in the sagittal plane of the fly: $F_{\text{total-x}}$ (the forces parallel to the longitudinal body axis) and $F_{\text{total-z}}$ (the forces perpendicular to the longitudinal body axis). Oscillations of the wire were damped with short foam cylinders placed at either end of the wire. The wire ran through the center of each cylinder, and the outer surface of the foam cylinders was compressed by a rigid brass covering. Mechanically induced oscillations of the tethered fly on the wire were damped in the horizontal and vertical directions to less than 30% between subsequent peaks. The damped oscillation is expected to increase the actual time constant of the force measurement from approximately 40 μs (see below) to approximately 56 μs. However, the oscillation and the oscillation-induced increment of the time constant can be almost completely reduced by off-line conditioning of the force records with an appropriate zero phase-lag filter.

Reconstruction of lift and thrust forces from the morphologically defined vectors, $F_{\text{total-x}}$ and $F_{\text{total-z}}$, depends upon the actual posture of a fly. A difference of 24° between the elevation angle of the mean force vector and the body angle of Drosophila has been determined using a mechno-electrical transducer by varying the body angle during tethered flight in still air (Götz and Wandel, 1984). The angle between the mean force vector and the body does not vary with the absolute orientation of the body in space, at least for the investigated range between −45 and +150° with respect to the horizontal, and is unaffected by visual stimulation (Götz, 1968). An effect of airspeed on the angle between the mean force vector and the body axis is conceivable, but difficult to assess. During free flight, D. melanogaster is thought to select its airspeed by controlling the body angle in the range between approximately 60° for hovering and approximately 30° for cruising in a narrow box of 50 cm diameter (K. G. Götz, unpublished results). An almost linear relationship between body angle and airspeed has been found in a larger congeneric species, D. hydei: 60° at 0 cm s⁻¹, 40° at 40 cm s⁻¹, and 20° at 80 cm s⁻¹ (David, 1978). During the fastest cruising flights in which the body axis is approximately aligned along the horizontal axis, $F_{\text{total-x}}$ would correspond to thrust and $F_{\text{total-z}}$ would correspond to lift. During hovering flight, when the animal maintains its body at an angle of about 60° with respect to the horizontal, the thrust component becomes very small and the upward lift becomes the resultant of $F_{\text{total-x}}$ and $F_{\text{total-z}}$.

**Interpretation of interferometric data**

The attempt to record small flight forces with a high temporal resolution confronted us with a series of challenging problems. We provide a short account of the physical assumptions underlying our interferometric methods to convey a feeling for the dimensions of the signals and the reliability
of their measurement. The interferometer was calibrated, for each of the 16 flies, by repeated application of horizontal and vertical forces of 100µN. However, time-variant flight forces resulting from a 190Hz wingbeat are not necessarily transformed into equivalent deflections of the wire. These forces act against (i) inertial forces proportional to acceleration, (ii) frictional forces proportional to velocity and (iii) elastic forces proportional to the position of both the fly and the wire. A deflection of the taut wire by a force of 10µN (roughly the weight of a Drosophila) resulted in a displacement of 2.9 nm, which corresponds to the length of a chain of 13 iron atoms in the wire. By using these values in an ordinary model of string mechanics, we estimated the time constant describing the transition to a new equilibrium to be 40µs. Calculation of the actual time course of a deflection shows that the wire should approach asymptotically to within 1% of its equilibrium position in less than 1.7% of an average wingbeat period of 5.26 ms. For this reason, the inertial forces resulting from the deflection of the combined wire and fly mass can be neglected. The same holds for the frictional forces. The frictional coefficient of a fly is approximately 4 mg s⁻¹, estimated from the ratio of body weight to maximum falling velocity of an anesthetized fly with its wings spread. Assuming that this term dominates the drag of the fly–wire system, the resulting frictional force (the product of the frictional coefficient and velocity) is nearly five orders of magnitude smaller than the weight of the fly. These results allow us to derive the time course of the flight force directly from the deflection of the wire. In the absence of further complications, the time resolution should be limited primarily by the resonance frequency of the system.

However, two dynamic artifacts of the interferometer must be discussed in order to interpret the interferometric measurements properly. (i) We observed a permanent low-amplitude modulation of the force components in the region of 2.8 kHz that was not correlated with the tension or deflection of the wire. This has tentatively been attributed to a vibration of the shims and was easily suppressed by averaging several wingbeat cycles. (ii) A transient resonance at approximately 1.8 kHz was observed following deflection of the wire. This effect shows a high degree of damping and is inconspicuous in the absence of an attached fly. The effect was greatest when a flying or resting fly was mounted onto the wire and the wire was deflected at an oblique angle relative to the animal’s body axis. The modulation frequency of this artifact did not increase significantly with the tension of the wire. These results suggest that this 1.8 kHz phenomenon results from a damped oscillation of the tethered fly around the axis of the wire. We calculated the expected initial deflection due to a change in the flight force acting on the center of gravity, the resonance frequency of the excited oscillation and its repulsive action on the wire. Our estimates are comparable with the observed artifact. In principle, this artifact could be avoided (i) by shortening the distance between the center of gravity of the fly and its point of attachment to the wire, or (ii) by increasing the stiffness in torsion of the wire at the expense of sensitivity. So far, both approaches have proved technically impossible to implement, and the flight force recordings are potentially contaminated by this artifact. A conspicuous 1.8 kHz oscillation did regularly appear in our recordings of the horizontal force component, \( F_{\text{total-x}} \), during the upstroke (see Fig. 10A). This oscillation should be considered with caution, since it is likely to represent the reverberation of the fly’s body mass around the wire rather than actual temporal fluctuations in flight forces. However, the 1.8 kHz reverberation can be treated as a contribution from an independent oscillator that is linearly superimposed onto the recorded flight forces and whose time average is zero. Estimates derived from a mathematical model of the fly–wire system suggest that the time constant of our force measurements (approximately 56 µs) is not significantly lengthened by superposition of the comparatively slow oscillation. In some analyses, we attenuated the influence of the 1.8 kHz oscillation by off-line conditioning with an appropriate zero-phase filter. This procedure removes the contribution of the contaminating reverberations, but diminishes the temporal resolution of our measurements by a factor of about two. This filtering is only justified if the force sensor is sufficiently linear so that its output remains balanced following superposition of large amplitude oscillations. In the present experiments, linearity up to at least 200 µN was achieved by operating the wire at high tension so that its displacements were extremely small. In summary, we believe that the interferometer provides a sufficiently accurate and instantaneous record of flight forces at frequencies below 1.8 kHz.

Results

Gross structure of wake

Several important features of the wake structure are manifest in the long-exposure images. For reference, a cartoon reconstruction of the generation of a single vortex ring is shown in Fig. 8. The individual vortex loops generated during each wing stroke progress downwards, tracing the outer boundary of the wake which appears as an outer layer of vortical flow in the sagittal images of Fig. 2A–E. Inside the vortical layer, there is a central region of high-velocity linear flow that is formed from the central portions of the individual vortex rings. We term the structure traced out by the rearward-moving vortex loops the vortex stack. As indicated in coronal sections (Figs 2F–J, 3), the cross section of the vortex stack near the fly is not circular, but rather has the outline of an inverted heart. The presence of a heart-shaped vortex stack is important because it provides evidence for the mechanisms of vortex shedding during the ventral reversal. As the wings rotate and change direction at the start of the upstroke, they rapidly shed vorticity along their lengths, leaving behind two vortex filaments that are continuous with the filaments shed during the downstroke (see Fig. 8). In many birds and insects that clap their wings at the bottom of the downstroke, the free distal ends of these vortex filaments fuse below the body to create a continuous circular vortex ring. The same is true for insects.
whose wings do not clap at the end of the downstroke (Grodnitsky and Morozov, 1992, 1993). Although the wings of *Drosophila* also reverse direction while still separated by a large ventral angle, the shed vortex filaments do not immediately fuse, but rather attach temporarily to the body. As the individual vortex loops move backwards, their ventral attachment points slide rearwards along the body towards the tip of the abdomen. In *Drosophila*, the section cuts a long tangent through the vortical layer with only a small portion that slices through the central region of the vortex stack. In *Drosophila*, the laser section just glances the lateral extent of the vortical layer. The section shown in *Drosophila*, 1 mm lateral to the wingbeat envelope, is outside the border of the vortical layer. (F,G) Coronal sections of the wake seen from behind. Anterior to the head (F), there is no evidence of the fly’s wake. The section through the wingbeat envelope near the wings’ position at the time of the ventral flip (G) shows the ventral boundary of the vortex stack. Note that the medial boundaries of the vortex stack are attached to the thorax of the fly. In *Drosophila*, the ventral boundaries of the vortex stack move downwards, but are still attached medially to the body. In the most posterior section (J), the dorsal boundary of the vortex stack is now visible, and the ventral attachment sites have slid off the tip of the abdomen. Scale bar, 1 mm.

**Dynamics of vortex ring formation**

After reconstructing the basic shape of the vortex rings from the long-exposure particle trajectories, we will now describe the formation of individual rings as visualized by short-exposure images of particle flow. All images were consistent with the formation of a single vortex ring made up of vorticity generated and shed during the downstroke and ventral flip. In this respect, the wake of a fruit fly is more similar to the general insect model described by Grodnitsky and Morozov (1992, 1993) than to the linked chain pattern described by Brodsky (1991, 1994). The clearest evidence for a single vortex ring is seen in phase-reconstructed films taken from a lateral sagittal plane, half the distance between the tip and base of the wing.
Wake and forces of a fruit fly

The flow moving rearwards from the stroke plane consists of long parallel particle streaks alternating with dark regions that are almost completely void of particles. These dark regions were very conspicuous features of our flow visualizations and could not be explained by shadows within the laser sheet or the inability to visualize rapidly moving particles. Whenever the fluid containing a uniform distribution of spores is accelerated, the particles should lag behind the surrounding air because of their greater density. Therefore, we interpret the dark areas as representing recently accelerated regions within the wake such as the high-velocity central portions of individual vortex loops. This interpretation is supported by the flow pattern at the dorsal and ventral boundaries of the dark segments in Fig. 4 (arrow in frame d5). The air flow constricts while passing through the dark regions, which is to be expected if the dark regions lie close to the plane of the vortex ring. Further, the dark regions originate behind the trailing edge of the wing during the downstroke and enlarge during the ventral flip (Fig. 4, frames d4–u1). No comparable dark, high-velocity region is generated during the upstroke (Fig. 4, frames u1–u3), although the particle visualization may not be sensitive enough to detect weak vorticity. We conclude that one vortex loop is created during each stroke and that it consists primarily of the tip vorticity shed gradually during the downstroke together with the vorticity shed rapidly along the lengths of the wings during the ventral flip. An upstroke vortex loop, if present, is certainly much weaker than the downstroke loop and could not be unambiguously resolved by our methods. Fig. 5 shows a cartoon tracing of this interpreted pattern of vortex loop formation from a selection of frames in Fig. 4.

The rapidity with which vorticity is shed during the ventral flip is most clearly seen in phase-reconstructed images of particle trajectories in a coronal plane through the anterior portion of the thorax (Fig. 6). As the wings rapidly supinate (Fig. 6, frames d5–u1), regions void of particles develop below the wings, bordered ventrally by parallel arrays of long downwardly directed particle streaks. These dark particle voids, now viewed from the rear, are the same as those seen moving backwards in the sagittal plane visualizations (Fig. 4) and indicate the high-velocity flow through the center of the vortex loops, now oriented outwards from the plane of the image. Following the ventral flip, the dark sections representing central portions of the vortex rings move rearwards out of the plane of section (Fig. 6, frames u2–dr). During most of the wing stroke, there is no indication of vorticity anterior to the wing hinge. Given the dramatic accelerations of the fluid during the ventral flip, it would appear that the strength of the vorticity shed from the wings during this rotation is greater than the tip vorticity shed during the downstroke. It is possible, however, that this impression is an artifact caused by the plane of section.

Fruit flies and other small insects are known to display ‘squeeze, clap and fling’ kinematics during the dorsal stroke reversal (Weis-Fogh, 1973; Ellington, 1984b; Götz, 1987). The flows generated by this behavior influence the wake structure by modulating the fluid velocity above the body in the central portion of each vortex loop (Fig. 7). The resolution of our images is not precise enough to determine the exact changes in flow induced by the dorsal closure of the wings, but the squeeze and clap kinematics appear to have important...
consequences for the periodicity of fluid velocity over the body. First, during the upstroke, the velocity of air over the dorsal surface of the body appears to increase as the area between the wings rapidly decreases (Fig. 7, frames vf–u2). This effect is probably due simply to the law of continuity – increased fluid velocity in a smaller cross-sectional area. Second, just prior to the clap, the close proximity of the two leading edges of the wings presents an instantaneous barrier to flow over the sagittal midline (Fig. 7, frame u3). This transition in flow from an initial increase to an eventual decrease in speed as the wings draw closer together is reminiscent of the ‘paddle or rake’ mechanism described by Cheer and Koehl (1987) for copepod feeding. Finally, during the clap, the closure of the trailing edges of the wings squeezes fluid rearwards, increasing the velocity of air over the thorax and abdomen (Fig. 7, frames dr, d1). Taken together, the dorsal stroke reversal appears to generate a more pulsatile flow over the body.

The flow visualizations indicate several important differences between the wake of a tethered fruit fly and the simple schematic wakes proposed by vortex models of flight (Rayner, 1979b; Ellington, 1984c). Within a simple circular vortex ring, there is one central region through which the linear velocity of the fluid is high. Inside the heart-shaped vortex loops of a fruit fly, the velocity distribution is more complex because the central region may be roughly subdivided into three flow corridors (Fig. 8). The midline dorsal corridor originates above the body and follows the outline traced by the wing tips. The velocity of air flow within this corridor is probably increased by the squeeze and clap kinematics of the wings. The large ventral angle between the wings during the ventral flip ensures that the filaments of shed wing vorticity will not fuse but rather attach to the body, enclosing the two ventral corridors of high-velocity flow bounded medially by the body. The existence of the three flow corridors immediately behind the stroke plane has been verified by Lehmann (1994) in a three-dimensional reconstruction of a fruit fly’s wake using hot-wire anemometry. This complex structure of the wake may be related to the flight control capabilities of the animal, since the presence of two lateral flow corridors indicates that the force-generating capabilities of the two wings are at least partially independent. Indeed, in the study mentioned above, Lehmann found that the relative velocity in the two lateral corridors changes during visually induced turns or when a specific steering muscle (the second basalar) was stimulated. His measurements also indicated that the three corridors eventually coalesce into a single circular section 5 mm posterior to the stroke plane. Quantitative measurements of the flow velocity within the wake are shown in Fig. 9, in which...
the streak lengths of the images in Figs 4 and 7 have been used to construct a map of average fluid velocity and flow streamlines in two sagittal planes. The central axis of the wake is oriented at approximately 25° with respect to the longitudinal body axis, which is consistent with the 24° elevation of the mean flight force vector measured by Götz and Wandel (1984). The velocity gradient across the body over the sagittal midline is quite large, and the resultant pressure differential could potentially act as a source of body lift (Fig. 9A, B). However, using our flow measurements, we estimate the pressure differential across the body to be approximately 0.07 N m\(^{-2}\), which would produce a body lift of only 0.13 μN or approximately 1% of the total body weight. This is a very rough estimate, however, based on a time average of the flows and must be considered with caution. The velocity map in a more lateral sagittal plane (Fig. 9D) shows a longitudinal section through one of the ventral corridors. The peak flow velocity appears lower than that over the sagittal midline, but this is probably an artifact due to the inertia of the visualization particles within the highly time-variant flow of the lateral corridors. The \textit{Lycopodium} spores should not accelerate to the peak air velocity because of their greater density. In addition, the inertia of the particles may make them accumulate in the outer vortical layer. The resultant paucity of particles within the dark regions decreases the accuracy of the interpolation algorithm used to reconstruct the velocity flow field.

Measurement of total flight forces

Using laser interferometry, we were able to measure the instantaneous net flight forces produced by tethered flying \textit{Drosophila} (Fig. 10). In order to construct both the magnitude and the orientation of the net force vector generated by the flies, we simultaneously recorded the force components parallel and perpendicular to the longitudinal body axis \((F_{\text{total-x}}, F_{\text{total-z}},\) respectively). To improve the signal-to-noise ratio and to sample over an extended time period, we superimposed an average of 987 sweeps of every nineteenth stroke cycle in each of 221 flight sequences from 16 flies. The signal-averaging was possible by triggering on the ventral flip timing pulse that was generated by the wingbeat processor. In total, the results represent approximately 6 h of flight on the interferometer. The timing pulse was also used to trigger a stroboscope after a variable delay. This allowed us to inspect the kinematics of the dorsal reversal and to measure its timing (Götz, 1987). To ensure that the averaging procedure did not obscure temporal relationships, we limited our quantitative analysis to long stable flight sequences with less than 3.5% variation in wingbeat frequency. The average wingbeat period of the sequences that met this criterion was 5.26±0.26 ms (S.D.). In order to average separate flight sequences together, we normalized the time base of each record to the wingbeat period.

We attempted to measure the magnitude of the mean flight force by abruptly terminating each flight sequence using a fine probe to obstruct the wing path. However, this procedure resulted in a force offset that was of comparable magnitude to the mean flight force. The offset arose because the mechanical force required to stop the fly (which was much greater than the peak magnitude of the flight force) caused the ends of the wire to catch on the damping foam. However, the relaxation time of the unwanted offset was larger than the cycle time by at least three orders of magnitude. This allowed us to separate, by computer-aided subtraction of the mean values of \(F_{\text{total-x}}\) and \(F_{\text{total-z}}\), reliable measurements of the fluctuation of these forces within a stroke cycle from less reliable measurements of their means. Without the necessity for excessive temporal resolution, the mean forces can be most accurately determined using the mechano-electrical transducer mentioned in an earlier section (described in Götz and Wandel, 1984). The
Fig. 6. Phase-reconstructed images visualized in coronal sections through the wingbeat envelope near the position of the wings at the time of the ventral flip (position G in Fig. 1C; see also the corresponding section in Fig. 2). The sequence of images is roughly equivalent to those shown in Fig. 4. The wake is viewed from the rear through a window in the flow tunnel. During the downstroke (d1–d5), the wings move forwards but do not greatly alter the flow within the plane of visualization. During the ventral flip (vf), the fluid accelerates as vorticity is shed along the wings. Notice that, in this particular image, the left wing rotates slightly in advance of the right wing. Just after the ventral flip (u1), the wings have supinated and begun to move rearwards out of the plane of section. The ventral boundary of the vortex stack is now visible just below the two dark regions under each wing. The lateral boundaries of the vortex stack are evident in the rotational flow present at the tips of the wings. During the upstroke and dorsal reversal (u2–dr), the wings move out of the plane of visualization, as do the dark regions representing the two lateral corridors of high-velocity fluid within the vortex stack. Scale bar, 1 mm.

Fig. 7. Phase-reconstructed images of the flow visualized in the mid-sagittal plane illustrating the squeeze, clap and fling behavior (position A in Fig. 1C; see also the corresponding section in Figs 2 and 3). Again, the sequence of images is approximately equivalent to those shown in Figs 4 and 6. Note that in all sections there is a large velocity gradient across the dorso-ventral axis of the fly. After the squeeze (d1), the leading edges of the wing are first to leave the plane of visualization as the wings peel apart. A new vortex loop develops as the wings move apart (d2). In frame d3, dark regions at the positions of the developing and recently shed vortex loops are especially clear (asterisks). At mid downstroke (d4), the wing has moved out of the plane of visualization. From the end of the downstroke to the start of the upstroke (d5–u2), the vortex loop moves backwards at a velocity of approximately 0.4 m s$^{-1}$ as indicated by the dark region above the body. During the clap (u3, dr), the wings are clearly visible above the dorsal midline. The fluid velocity between and behind the wings becomes small, presumably as a result of the obstruction caused by the close apposition of the leading edges. The fluid velocity behind the wings greatly increases as the trailing edges squeeze together (dr). Scale bar, 1 mm.
The magnitude of the mean force vector, recorded under the conditions of both the flow visualization and the interferometer experiments, was $10.8 \pm 0.5 \mu N$ (S.E.M., 74 sequences from 17 flies) in still air and $10.4 \pm 0.4 \mu N$ (S.E.M., 90 sequences from 19 flies) in a $20 \text{ cm s}^{-1}$ air flow. Since the forces measured in still and moving air were not significantly different (Fig. 10A), we pooled the data, yielding a total mean of $10.6 \pm 0.3 \mu N$. This force is the equivalent of the average body weight of a female *Drosophila*. As mentioned above, the elevation angle of this vector in the $x-z$ plane is approximately $24^\circ$. The corresponding components of the mean flight force amount to $9.7 \mu N$ for $F_{\text{total-x}}$ and $4.3 \mu N$ for $F_{\text{total-z}}$. In the following analyses, these values replace the less reliable mean flight forces obtained using the interferometer. All of the 16 flies were tested alternately in still air and in the presence of a $20 \text{ cm s}^{-1}$ air flow identical to that used in the flow visualization experiments. As shown in Fig. 10A, the differences in the time course and magnitude of the force measurements under these two conditions were small compared with the variation among individuals. The similarity of the force records holds for each of the 16 flies and is not unexpected considering that a background air flow of $20 \text{ cm s}^{-1}$ produces an effective advance ratio of only 0.085. The close coincidence of the two independent data sets throughout the stroke cycle demonstrates the rigorous reproducibility of the interferometric force measurements and allowed us to pool the results for further evaluation. The magnitude and time history of forces measured in these experiments were consistent across averaged sequences. The limiting curves in Fig. 10A represent the standard deviation (S.D.) of the pooled data from 221 flight sequences. The corresponding standard errors (7% of the S.D.) and the 95% confidence limits (13% of the S.D.) of the means are too small to be represented graphically.

As seen in the $F_{\text{total-x}}$ waveform in Fig. 10A, the forces developed during the ventral flip appear transiently to drive the fly on the wire to a resonance of about $1.8 \text{ kHz}$, which is a factor of 0.45 lower than the resonance frequency of the tuned wire with an attached fly. Tapping the wire elicits a similar oscillation, regardless of whether the animal is flying. For this reason, these oscillations do not seem to be attributable to flight-associated periodic processes such as rapidly changing aerodynamic forces or inertial forces resulting from rotation or deformation of the wing during the ventral flip. The extreme angular acceleration and deceleration during the ventral flip is likely to exceed $\pm 3 \times 10^8 \text{ degrees s}^{-2}$ (see Fig. 6b in Zanker and Götz, 1990). Conservation of the angular momentum requires the induction of torque pulses of up to $4 \text{ nN m}$ about an axis parallel to the wire. The time course and magnitude of either these pulses or the compensatory forces (which may exceed $5 \mu N$) appear to be sufficient to induce the observed oscillatory reaction of the wire. Whether elicited by flight forces or rotational momentum, the $1.8 \text{ kHz}$ oscillations...
are not likely to represent the time course of changing aerodynamic forces and have been filtered in the reconstructions presented in Fig. 11.

The time courses of the total flight force records in Fig. 10A are qualitatively similar to those recorded by G. Nalbach (resonance frequency 2 kHz; unpublished results) for Calliphora erythrocephalia, but quite different from those published for Sarcophaga bullata (Buckholz, 1981). Buckholz attached his flies to a copper wire of low tensile strength and recorded the orthogonal components of a just-visible vibration by measuring reflected light. From the data presented in his paper, we estimate that the time constant for the asymptotic transition to a new equilibrium is at least two orders of magnitude larger than that in the present experiments. The resulting effects of inertia and friction complicate the interpretation of his data and may explain the large discrepancy between the results.

Reconstruction of aerodynamic forces

The raw signals transduced by the sensor attached to a fly’s thorax represent the sum of aerodynamic and inertial forces ($F_{\text{total-x}}$ and $F_{\text{total-z}}$). The inertial forces ($F_{\text{inert-x}}$ and $F_{\text{inert-z}}$)
result when the mass of the animal’s wings and the added mass of the surrounding air are accelerated during the wing stroke. While the inertial forces averaged over an entire wing stroke are zero, they are transiently quite large and must be subtracted from the total measured forces in order to reconstruct the instantaneous aerodynamic forces ($F_{\text{aero}}-x$ and $F_{\text{aero}}-z$). Zanker and Götz (1990) have previously calculated the inertial forces using the data of Zanker (1990a), which were based on reconstructed kinematics of 25 phase-equidistant points within the wing stroke. We interpolated these calculated waveforms to match our sampling rate (100 points per wingstroke) by using a cubic spline function (Fig. 10B). Before subtraction, the two data sets were aligned, matching the extreme downstroke position in Zanker’s data with the timing of the ventral flip pulse in the force recordings. However, it should be noted that the accuracy of the temporal alignment is limited by the 200μs effective sampling interval of the kinematic data. In addition, the reconstruction of aerodynamic forces by inertial subtraction requires several simplifying assumptions. (i) The inertial forces were calculated from averaged wing-stroke kinematics. This may have a smoothing effect on the time course. Note, however, that the same holds true for the averaged time course of the recorded flight forces. (ii) Inertial force components due to pronation or supination of the wings were neglected. This is justified only in the case of rigid wings and a sufficiently symmetrical distribution of the total wing mass around the axis of rotation. (iii) The inertia resulting from the mass of the wing and the virtual mass of the bound air cannot be determined with sufficient accuracy. As a small fraction of the resulting mass, the virtual mass has been replaced in the calculation by a point mass near its estimated center of gravity on the wing. In order to assess the inaccuracies that might be introduced by these assumptions, we varied the magnitude of the inertial force trajectories used in the reconstructions of aerodynamic forces. As indicated in Fig. 10C, the calculated aerodynamic forces are qualitatively similar when using inertial force magnitudes of 75%, 100% and 125% of those calculated by Zanker and Götz (1990). Thus, although the unknown contribution of rotational inertia remains a potential source of error, it is unlikely that our reconstructions would be compromised by serious inaccuracies in the estimation of the magnitude of translational inertia. According to earlier estimates (Zanker and Götz, 1990), the time course of the total flight force is expected to resemble the time course of its dominant component, the inertial force. Comparison of the corresponding curves in Fig. 10B illustrates the expected similarity. Evaluation of the actual data corroborates this impression: the correlation cannot be significantly improved by varying the magnitude and phase of the curves calculated by Zanker and Götz (1990) for the inertial forces. It is not easy to explain this coincidence if the corresponding forces were not measured or calculated with sufficient accuracy in their magnitude and phase.

The orthogonal aerodynamic forces were used to reconstruct trigonometrically the time history of the direction and magnitude of the total aerodynamic force generated by a flying Drosophila (Fig. 11A). Because high frequencies within the signals do not represent components of the flight forces, we have also plotted low-pass-filtered versions of the data records. The magnitude of aerodynamic forces within each wing stroke oscillates between segments of high and low force generation. The total flight force rises to a plateau of approximately 35μN during the downstroke and then falls during the second half of the upstroke. There appears to be a transient peak in the unfiltered version of the reconstructed flight force during the upstroke which exceeds 80μN although, as discussed previously, this is probably an artifact due to the 1.8kHz oscillation around the axis of the wire. The fluctuations in force magnitude are in phase with large changes in the orientation of the force vector. The largest flight forces are oriented roughly forward along the body axis. In contrast, the low-magnitude flight forces during the late upstroke and early downstroke are oriented upward and rearward.

The body of a free-flying Drosophila moving at 20 cm s$^{-1}$ should be inclined at an angle of approximately 50° with respect to the horizontal (David, 1978). In Fig. 11B, we have reconstructed the time histories of the lift and thrust vectors under these free-flight conditions on the basis of our interferometric measurements. Again, we show both filtered and unfiltered versions of the reconstructed waveforms. With the body inclined at 50°, the wings generate upward lift from the middle of the downstroke to the end of the upstroke. Lift then declines to small negative values during the start of the downstroke. Thrust, by contrast, oscillates between nearly equal positive and negative extremes. Thrust is negative (rearward) from the end of the upstroke to the middle of the downstroke, at which time it rises quickly (within 0.9 ms) to a peak positive value of approximately 30μN. Thrust subsequently declines during the upstroke to reach a peak negative value by the start of the downstroke. The mean lift and thrust values at an inclination of 50° are 10.2 and 3.0μN respectively.

On the basis of the flow visualizations, the largest flight forces are expected to occur during the downstroke and ventral flip when the wings appear to generate the most circulation (Fig. 6). However, from the traces in Fig. 11, it is clear that measured forces are greatest from the middle of the downstroke to the end of the upstroke. Thus, the measured flight forces are delayed by about 1 ms with respect to our expectations based on the flow visualizations.

**Discussion**

Any coherent theory of animal flight must be able to integrate the dynamics of wake formation with the dynamics of force generation. In this study, we have attempted to correlate the instantaneous aerodynamic forces produced by a fly with the time history and structure of its vortex wake. In each wing stroke, the fly produces a single heart-shaped vortex loop that is composed of vorticity generated and shed during the downstroke and ventral reversal. The wings appear to shed
little or no vorticity during the upstroke. In this way, the wake structure is similar to that previously reported for birds (Kokshaysky, 1979; Spedding et al. 1984; Spedding, 1986) and some insects, including the house fly *Musca domestica* (Grodnitsky and Morozov, 1992, 1993). However, the wake of a fruit fly differs from all previous descriptions of single-loop
wakes in that the ventral ends of the vortex ring do not immediately fuse above or below the body of the insect, but instead attach separately on either side of the thorax. Only after sliding along the fly’s body to the tip of the abdomen do the two ends of the vortex loop fuse to form a complete ring. The pattern of vortex formation would predict that the aerodynamic forces produced by fruit flies oscillate throughout the wing stroke – with a large force corresponding with the enlargement of the vortex ring during the downstroke and ventral flip, and little force being generated during the upstroke. The results of laser interferometry partially verify this prediction. The aerodynamic forces do indeed oscillate, yet the measured forces lag behind their expected temporal position by approximately 1 ms, corresponding to about one-fifth of the stroke cycle. In the following discussion, we will attempt to synthesize these two observations in order to present some plausible models for the mechanisms of force generation by Drosophila.

**Force generation during the wing stroke**

On the basis of the flow visualizations, it appears that the fly generates a vortex loop composed of the vorticity shed during the downstroke and ventral reversal. The strength of this vorticity may be estimated by relating the changes in fluid momentum to the corresponding aerodynamic forces. The momentum of a vortex ring, \( M_v \), is equal to \( \rho A \phi \), where \( \rho \) is air density, \( A \) is ring circulation (using the nomenclature of Spedding et al. 1984) and \( A \) is the area of the vortex ring (Milne-Thomson, 1966). As shown by the wake visualizations, the vortex rings of the fly enclose the area swept by the two wings within their stroke plane. Thus, we may estimate the momentum of the fly’s vortex ring as:

\[
M_v = \rho A \phi R^2, 
\]

where \( \phi \) is the angular position of the wing in radians and \( R \) is wing length. Differentiating equation 1 with respect to time yields \( F_v \), the force resulting from the change in fluid momentum associated with a single vortex:

\[
F_v = \frac{dM_v}{dt} = \rho R^2 \frac{d(\phi \phi)}{d\phi}. 
\]

In the simplest model of stroke kinematics, the two wings start together \( \theta(0)=0 \) with no bound circulation \( \kappa(0)=0 \). Solving for \( \kappa \) under these conditions yields:

\[
\kappa(t) = \frac{\tau}{\phi(t)R^2} \left[ \frac{1}{2} \int_0^t F_v(t)dt \right]. 
\]

The quantity in brackets is simply the average force, \( F_v \), from time \( t=0 \) to \( t=t \). The circulation, \( \kappa_s \), at the end of a stroke of duration \( t_s \), is given by:

\[
\kappa_s = \frac{t_s}{\Phi} \frac{1}{\phi(t)R^2} F_v, 
\]

where \( \Phi \) is the full stroke amplitude. This equation provides a means of calculating the ring circulation generated during a single stroke from the average force and simple kinematic parameters. Estimates of ring circulation based on our force measurements are given in Table 1. On the basis of the flow visualization results, the ring circulation should correspond only to the forces generated during the downstroke and ventral reversal.

<table>
<thead>
<tr>
<th>Force model</th>
<th>Stroke time (ms)</th>
<th>Average force (( \mu N ))</th>
<th>( 10^3 \times \text{ring circulation}, \kappa ) (m(^2) s(^{-1}))</th>
<th>( 10^0 \times \text{ring momentum,} M_v ) (kg m s(^{-1}))</th>
</tr>
</thead>
<tbody>
<tr>
<td>Downstroke</td>
<td>3.47</td>
<td>19.9</td>
<td>3.83</td>
<td>69.1</td>
</tr>
<tr>
<td>average</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Upstroke</td>
<td>1.79</td>
<td>28.2</td>
<td>2.80</td>
<td>50.5</td>
</tr>
<tr>
<td>average</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Full stroke</td>
<td>5.26</td>
<td>22.6</td>
<td>6.60</td>
<td>118.8</td>
</tr>
<tr>
<td>average</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Average force at 24° elevation</td>
<td>3.47</td>
<td>10.6</td>
<td>2.06</td>
<td>37.2</td>
</tr>
</tbody>
</table>

The stroke durations were based on the mean wingbeat period (5.26 ms) and the average downstroke–upstroke duty cycle of approximately 2:1.

The values of wing length (2.47 mm) and stroke amplitude (2.46 rad) were taken from Zanker (1990a).

As explained in the text, the calculations are bracketed by using four different estimates of \( F_v \). The calculations of average force at 24° elevation are based on our measurement of the mean flight force and the work of Götz and Wandel (1984), who found that the mean force vector is invariably oriented at an angle of 24° with respect to the longitudinal body axis.

The weight of a typical Drosophila melanogaster is about 10 \( \mu N \).
flip. Averaging the force record in Fig. 11 over the downstroke interval yields a ring circulation of $3.83 \times 10^{-3}$ m$^2$ s$^{-1}$. Although inconsistent with our flow visualizations, ring circulation that would result from the average upstroke force is $2.80 \times 10^{-3}$ m$^2$ s$^{-1}$. However, because of the unexplained temporal shift in the periodic aerodynamic forces relative to

Fig. 11. Reconstruction of total aerodynamic force as well as lift and thrust vectors for a slowly flying animal. (A) The magnitude and direction of net aerodynamic force vectors were calculated trigonometrically from the $F_{aero-x}$ and $F_{aero-z}$ traces shown in Fig. 10C (using the 100% values of the inertial forces for subtraction). Because of potential contamination by superimposed oscillations at higher frequencies (see text), the filtered (thick line) and unfiltered (thin line) versions of each waveform have been plotted. We used a fourth-order zero phase-lag digital Butterworth filter with a cut-off frequency of 1.5 kHz. The magnitude of the flight force vector grows during the downstroke and starts to decay during the upstroke, with the peak forces oriented primarily along the axis of the body. (B) Using the same data, the lift and thrust have been reconstructed for an animal flying with a body angle of 50° with respect to the horizontal, a posture expected for animals in forward flight at 20 cm s$^{-1}$. As in A, both filtered and unfiltered versions of the data are shown. Both lift and thrust are positive from the late downstroke to the late upstroke. During the early part of the downstroke, lift production is zero, while thrust is negative. vf, ventral flip; dr, dorsal reversal.
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the stroke kinematics, we cannot be confident that the reconstructed forces for either stroke correspond strictly to the intervals of vortex loop formation. Nevertheless, we can make reasonable estimates of the range of values. A liberal estimate of ring circulation would be obtained by using the average force during both the upstroke and downstroke (22.6 μN) and assuming that it was generated over the entire wingbeat period. This procedure yields a ring circulation of 6.60 × 10^{-3} m^2 s^{-1}. A more conservative estimate would be obtained by using the magnitude of the mean force vector (10.6 μN) and assuming that it was produced entirely during the downstroke. This set of assumptions yields a ring circulation of 2.06 × 10^{-3} m^2 s^{-1}. Thus, the estimated ring circulation generated by a flying fruit fly falls somewhere between 2 × 10^{-3} and 7 × 10^{-3} m^2 s^{-1}. At first glance, these values appear small, being roughly three orders of magnitude lower than that predicted for a slowly flying pigeon (1.79 m^2 s^{-1}; Spedding et al. 1994). However, given the dimensions and velocity of a *Drosophila* wing during flight, even a value as low as 2 × 10^{-3} m^2 s^{-1} could only be generated by aerodynamically efficient wings. The ring circulation should be roughly comparable to the bound sectional circulation of the wings. According to Kutta–Joukowski theory, the sectional lift coefficient of an airfoil is given by 2ρUc, where *U* is the wing velocity and *c* is the mean chord length (circulation, *κ*, in the Kutta–Joukowski equation is often denoted with the symbol Κ). Taking values of *U* = 1.25 m s^{-1} and *c* = 0.85 mm, from Zanker and Götz (1990), this predicts a lift coefficient of approximately 3.7, which would certainly require the operation of unsteady mechanisms. Such processes might include delayed stall and the presence of a leading-edge vortex (Spedding, 1992; Dickinson and Götz, 1993; Ellington, 1995). Although we saw no direct evidence for a leading-edge vortex, such a structure would probably be beyond the resolution of our visualization techniques. Ellington (1995) has succeeded in visualizing such a structure during the downstroke in *Manduca sexta* using a smoke rake, but only after much effort. Unlike the enormous structures that may be easily visualized on a two-dimensional model (Dickinson and Götz, 1993; Dickinson, 1994), the leading-edge vortices on an actual insect wing are likely to be small owing to the axial flow that should remove energy from the developing vortex (Maxworthy, 1979, 1981; Spedding and Maxworthy, 1986; Wu et al. 1991). On the basis of his experiments with *Manduca sexta*, Ellington and his colleagues (Ellington, 1995; Willmott, 1995; C. van den Berg and C. P. Ellington, in preparation) have argued that the magnitude of this length-wise flow can be quite large and may serve to stabilize the leading-edge vortices so that they remain attached for a longer translational distance. At the moment, this complicated process of dynamic stall, as it unfolds in three dimensions, is the most likely explanation for the enhanced circulation generated by the fly’s wings during the downstroke.

**Time course of force production**

There are several possible explanations for the discrepancy between our flow visualizations and force measurements. First, it is possible that the lag in the aerodynamic forces relative to the stroke kinematics was due to a phase delay caused by the dynamic properties of the interferometric sensor. However, as mentioned in an earlier section, it should take the wire no more than 90 μs to reach within 1% of its new equilibrium value following the application of a 10 μN force. Thus, the dynamics of the sensor cannot easily explain the temporal delay.

Second, the time course of the force transients might be an artifact caused by incorrect subtraction of the inertial forces required to reconstruct the aerodynamic components. As indicated in Fig. 10, varying the magnitude of the inertial force did not introduce substantial changes in the resultant time histories of the aerodynamic forces. Such inaccuracies might be responsible for differences in the magnitude of the calculated aerodynamic forces, yet under all conditions the maximum and minimum forces do not precisely align with the upstroke and downstroke. During stroke reversal, the flipping wings of *Drosophila* appear to rotate about their long axis. Asymmetry in the rotatory acceleration and deceleration of the wing mass on either side of this axis is inconspicuous when the wing kinematics are examined using a stroboscope. If present, such asymmetries could account for minor increments or decrements of the calculated inertial forces. The greatest effects are expected during the ventral flip and during the dorsal squeeze, clap and fling, where a reconstruction of the aerodynamic forces is particularly difficult.

The third explanation for the discrepancy between the flow visualizations and the force measurements is that the flow visualizations might not have provided sufficient temporal or spatial resolution to identify the shedding of tip vorticity during the upstroke. Some evidence for the presence of two vortex rings per stroke in the wakes of blowflies can be found in Wood’s (1970), anemometric study of *Calliphora erythrocephalia* and *Phormia regina*. Wood reported that the air velocity within the wake showed two distinct peaks, which he used as evidence to claim that forces are generated during both the upstroke and the downstroke. However, close inspection of his results indicates that the majority of his records, including those that were likely to sample the air velocity in the center of the fly’s wake, actually show a single velocity peak within each wing stroke. Further, because Wood flew his tethered blowflies within a 2 m s^{-1} air flow, his results are not directly comparable with the near-hovering conditions in the present study.

As reviewed by Ellington (1995), there is some controversy in the literature over whether or not tip vorticity is shed during the upstroke. While Brodsky’s (1991, 1994) wake reconstructions from flow visualizations of butterflies include tip vorticities shed during the upstroke, Grønditsky and Morozov (1992, 1993) did not observe comparable structures within the wakes of several insects, including bugs, flies, lacewings and two lepidopteran species. The absence of upstroke vorticity is also consistent with the patterns described for slowly flying birds (Kokshaysky, 1979; Spedding et al. 1984; Spedding, 1986) and bats (Rayner et al. 1986). Comparisons among species should be made cautiously, however, especially for fruit flies, which operate at both a higher wingbeat frequency and a lower
The Wagner effect and the absence of upstroke vorticity

The absence of upstroke vorticity, if true under certain conditions, begs a question: why do the wings not develop circulation during the upstroke? This is a general question that can be applied to hovering birds and other animals that produce a single vortex with each stroke. Several factors might contribute to the absence of upstroke vorticity. First, the angle of attack of the wing with respect to the local flow might be low during the upstroke. According to the kinematic reconstruction of Zanker and Götz (1990), the angle of attack during the upstroke in *Drosophila* is negative and slightly smaller in magnitude than the angle of attack during the downstroke. The negative angle of attack means that the oncoming air would strike the morphological dorsal surface of the wing, which should generate an upstroke vortex ring with a similar orientation to the downstroke ring. However, this calculation of the aerodynamic angle of attack was based on a stroke-averaged estimate of the induced velocity vector. As indicated by our flow visualizations, the velocity field around the wing is time-dependent, and the instantaneous angles of attack may be somewhat different from those calculated using a constant induced velocity term. Despite these possible inaccuracies, the angle of attack of the wings during the upstroke is undoubtedly negative, and any circulation generated would have the opposite sense to that produced during the downstroke. The durations of the two strokes are also quite different, as the downstroke accounts for just less than two-thirds of the entire wingbeat cycle. However, although this would mean that vorticity has less time to develop, the wing must travel the same distance during the upstroke and accomplishes this by traveling at a greater velocity. If anything, one would expect this increased velocity to result in greater circulation during the upstroke. Thus, neither differences in angle of attack nor stroke duty cycle can easily explain the apparent absence of upstroke circulation in *Drosophila*.

The most likely explanation for the absence of, or reduction in, circulation lies with the peculiar flow conditions at the start of the upstroke. In *Drosophila*, the downstroke begins with the intensely studied ‘squeeze, clap and fling’ motion (Weis-Fogh, 1973; Bennett, 1977; Maxworthy, 1979; Ellington, 1984b; Spedding and Maxworthy, 1986; Götz, 1987). The close apposition of the wing tips during this behavior serves to link the fluid mechanical processes of the two wings so that the bound vorticity of one wing constitutes the starting vortex of the other. As the wings separate, their tip vortices fuse and thus create the dorsal segment of the developing vortex loop. These conditions of close proximity are not repeated at the beginning of the upstroke, at which time the wings are separated by...

As discussed throughout this paper, both the flow visualizations and force measurements that we have presented are subject to error. Nevertheless, given the experimental challenges associated with the small size and high wingbeat frequency of *Drosophila*, we may have approached the limits of resolution that are currently available. A more satisfactory explanation for the apparent phase lag between our force records and flow visualizations may eventually emerge after the development of new measurement techniques or experiments with realistic physical models.
approximately 80°. This separation is too large for the exchange of vorticity, as shown by the lack of fusion between the shed vortex filaments after the ventral flip. At the start of the upstroke, two factors might inhibit the generation of circulation by the wings. First, their separation does not allow the swapping of starting and bound vorticity that operates at the start of the downstroke. Second, at the start of the upstroke, the wings begin translating in the presence of the large filaments shed during stroke reversal. These filaments consist of the stopping vorticity of the downstroke augmented by the shed rotational circulation generated during the ventral flip. This free vorticity would have the same sense as that of the starting vortex of the upstroke. The Wagner effect (Wagner, 1925) describes how the bound circulation of a wing starting from rest is delayed by the presence of its own starting vortex. In the case of fly wings at the start of the upstroke, this effect will be greatly amplified because each wing must separate not only from its own starting vortex but also from the large shed vortex of the previous stroke. This ‘additive-Wagner effect’ (Fig. 12) would greatly attenuate the development of bound circulation and could explain the absence of tip vortices and force generation during the upstroke. Evidence for such an effect may be seen in previous studies on unsteady aerodynamics mechanisms in two-dimensional model Drosophila wings (Dickinson and Götz, 1993; Dickinson, 1994). The generation of lift by the model was greatly attenuated when translation was preceded by a two-chord downstroke and rotation (Fig. 7A in Dickinson, 1994). When following a previous stroke reversal, the lift generated after two chords of travel at an angle of attack of 36° was nearly 3.5 times lower than that generated during an impulsive start from rest. This attenuation was critically dependent on the duration of the previous stroke, indicating that the sign of the attached vorticity shed by the previous stroke was an essential determinant of the effect’s magnitude. After two chords of translation at a high angle of attack, the initial leading-edge vortex was still attached to the model wing and, after shedding, had the correct rotational sense to inhibit the development of circulation in the subsequent stroke via the additive-Wagner effect. The attenuation is not present following a 7.5 chord downstroke, in which the leading-edge vortex has detached before rotation, replaced by a trailing-edge vortex of opposite sense.

The negative influence of one stroke’s circulation on the next is probably not exclusive to flies or other animals that perform a clap and fling. Rather, the proposed additive-Wagner effect might influence the design of kinematics in many animals that employ a reciprocating wing stroke. One consequence of the effect is that it may not be profitable to produce force during both the upstroke and downstroke, since the presence of circulation in one half-stroke will delay the generation of circulation in the next. Instead, the animal might do better by using one single power stroke, alternating with a non-circulatory recovery stroke. The lack of circulation during the recovery stroke ensures more rapid force generation during the power stroke. The effect might also explain the transition from the single vortex loop pattern seen in hovering animals to the more complicated linked vortex chains described by Brodsky (1991, 1994). As the advance ratio increases, the vorticity shed during the downstroke and ventral flip will move rearwards at an increasing rate relative to the velocity of the wings. At a certain point, the rearward velocity of the vortex loop will be fast enough so that the shed downstroke vorticity is far enough away from the wing to allow the formation of upstroke circulation. Under these conditions, the wake would take on the ‘linked-chain’ structure described by Brodsky (1991, 1994), in which the tip vortex filaments of each stroke are connected by common starting–stopping vortices at stroke reversal. In addition to the advance ratio, the transition from a discrete series of vortex rings to a linked chain would depend on many factors, including Reynolds number, wing separation and wing shape, all of which may contribute to the discrepancies already described in the flow visualizations of various insects.

We wish to thank Michael Renner for his extensive help with the acquisition and processing of the flight force measurements. Fritz-Olaf Lehmann and Roland Strauss also provided additional technical support during the execution of this work. The authors would also like to thank the many helpful and provocative comments of two anonymous reviewers. This work was funded in part by the Max Planck Gesellschaft, the David and Lucille Packard Foundation and NSF Grant IBN-9208765 to M.H.D.

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